



## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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<p>(21) International Application Number: PCT/NL97/00384 (22) International Filing Date: 4 July 1997 (04.07.97) (30) Priority Data: 1003527 5 July 1996 (05.07.96) NL (71) Applicant (for all designated States except US): B.V. OPTISCHE INDUSTRIE "DE OUDE DELFT" [NL/NL]; Postbus 72, NL-2600 MD Delft (NL). (72) Inventors; and (75) Inventors/Applicants (for US only): LÖFFLER, Edgar, German [DE/DE]; Bresserbergstrasse 72, D-47533 Kleve (DE). VISSCHER, Arie, Luite [NL/NL]; W. Banninglaan 33, NL-3972 SJ Driebergen (NL). (74) Agent: VAN DER BURG, Louis; B.V. Optische Industrie "De Oude Delft", Postbus 72, NL-2600 MD Delft (NL).</p>		<p>(81) Designated States: JP, US, European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).  Published With international search report. In English translation (filed in Dutch).</p>
<p>(54) Title: CATHETER</p> <div data-bbox="256 1125 1347 1344"> </div> <p>(57) Abstract</p> <p>A catheter provided with an elongated tube having channels for the guiding of a radioactive element and for the passage of a guide wire for the catheter as well as fluid under pressure, in which the elongated tube is provided near its distal end on its outer circumference with a recanalization balloon and activatable centering means arranged therein. A by-pass can also be arranged through the recanalization balloon.</p>		

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## CATHETER

The present invention relates to a catheter comprising an elongated tube having a first channel for the guiding of a radioactive element and a second channel for the passage of a guide wire for the catheter, the elongated tube being provided with temporarily activatable centering means on its outer circumference near its distal end.

Such a catheter known from EP-A-0 688 580 is intended for use after a recanalization treatment in which a substantially occluded blood vessel (for example as a result of the deposition of so-called plaque within the lumen of the blood vessel) is stretched by means of an expandable element such as a fluid-inflatable recanalization balloon, fastened at the distal end of an elongated catheter tube in order to permit the blood to flow unimpeded through the stretched blood vessel.

It is frequently found after a relatively short period of time that a new recanalization treatment is necessary because a constriction is again forming in the blood vessel or has already formed. The constriction may be a consequence of tissue developing at the stretched place (known as neointima proliferation), probably due to the fact that the wall of the blood vessel is damaged by the stretching. This formation of tissue can be prevented to a large extent, or at least reduced, if, during or shortly after the recanalization treatment, the blood-vessel tissue in question is irradiated with ionizing radiation, in particular  $\beta$  and/or  $\gamma$  radiation.

For such a treatment, the catheter known from EP-A-0 668 580 can be used. The intensity of radiation of the radioactive element introduced decreases greatly with the distance. In order not to permit the radiation dose to be too great (damaging of vessel wall) or too low (not the intended reduction of tissue developing at the stretched place), it is important to center the radioactive element accurately in the blood vessel. This is done in the known

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catheter by centering means in the form of an inflatable balloon which is subdivided by constriction means into a plurality of balloon parts. The constriction means are so dimensioned that the different balloon parts communicate  
5 with each other.

Upon such a treatment, therefore, the recanalization catheter must first of all be brought to the desired place and after the carrying out of the recanalization treatment, be removed and replaced by the  
10 catheter for the guiding of the radioactive element, in which connection, of course, great care must be paid to the fact that the radioactive element can be placed precisely at the place of the earlier recanalization treatment. All in all a cumbersome and timeconsuming method which must be  
15 carried out extremely cautiously, while, also from the standpoint of the patient who must undergo the treatment, it is preferable for it to be carried out as rapidly and efficiently as possible.

The object of the present invention thus is also  
20 the provision of such an instrument that the treatment can be carried out in a short time effectively and reliably with as few manipulations as possible.

This is achieved, in accordance with the present invention, by a catheter of the type described above in the  
25 manner that the centering means are surrounded by a recanalization balloon which is inflatable by a fluid introduced via a third channel so as to form an elongated body and in the manner that the centering means are activatable within the recanalization balloon. By these  
30 measures, the recanalization treatment and the irradiation treatment of the stretched region of the blood vessel can be carried out with one and the same catheter, in other words rapidly and without loss or time, since a catheter removal action and introduction action are avoided, which  
35 also is particularly valued by the patient. Furthermore, the fact that it is not necessary to change the catheter has the particular additional advantage that the centering

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means are automatically located at the precisely desired place so that, in addition, there is also obtained a guarantee that the radiation will always be carried out at the correct place as well as in the correct manner.

5           The activating of the centering means can in this connection be carried out both simultaneously with and by the inflating of the recanalization balloon as well as independently thereof, in particular after the carrying out of the recanalization treatment.

10           The activating of the centering means simultaneously with the inflation of the recanalization balloon can take place automatically if, in accordance with another embodiment of the invention, the centering means are connected, on the one hand, to the recanalization  
15 balloon and, on the other hand, to the tube, all in such a manner that the tube is centered in the recanalization balloon upon the inflation thereof. The centering means can, in this connection, consist, for instance, of a number of annular parts of thin plastic material which, for the  
20 introduction of the catheter, can be laid compactly around the tube together with the recanalization balloon around the tube, and by the inflation of the recanalization balloon, come into a position extending transversely on the tube in order thus to center the tube with respect to the  
25 recanalization balloon. Furthermore, the centering means can have wire-shaped parts which, in the inflated condition of the recanalization balloon, extend radially with respect to the tube.

          In accordance with another embodiment of the  
30 invention, it is also preferable for the centering means to comprise inflatable balloon means which are inflatable by fluid introduced via the third channel, the balloon means comprising a plurality of balloons which center the part of the first channel protruding between the balloons with  
35 respect to the recanalization balloon.

          If preference is given to the centering means being activatable independently of the recanalization

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balloon, for instance after the recanalization treatment has been completed, then, in accordance with a further embodiment of the invention, it is preferred that the centering means comprise inflatable balloon means which are  
5 inflatable by fluid introduced via at least a fourth channel arranged in the tube, in which connection the balloon means comprise a number of balloons which center the part of the first channel extending between the balloons with respect to the outer circumference of the  
10 recanalization balloon. The centering balloons may consist of a plurality of balloons arranged one behind the other along the tube or of a plurality of elongated balloons which lie radially alongside of each other around the tube.

The use of the same catheter for both the  
15 recanalization treatment and the irradiation treatment results in a longer continuous dwell time of the catheter at the place of treatment than in the case of two successively introduced catheters. In this connection, it is preferred in accordance with a further embodiment of the  
20 invention that a further channel be present which extends from a distal place past the recanalization balloon and the centering means to past the proximal end of the recanalization balloon and the centering means and is provided on opposite sides of the recanalization balloon  
25 and the centering means with at least one communicating opening with the surroundings. By these measures, the flow of the blood through the treated blood vessel can remain undisturbed to a far-reaching extent, which makes special measures with regard to this generally unnecessary. This  
30 effect can be realized in particularly advantageous manner if, in accordance with another preferred embodiment of the invention, the further channel coincides with the second channel, in which case the guide wire can be pulled further back from the distal end of a second channel than the  
35 proximal connecting opening or openings. Therefore, use is made in advantageous manner of the existing channel for the

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guide wire, as is directly possible since the guide wire, after bringing the catheter to its place, has no further active function to perform and can be withdrawn without problems into a waiting state.

5           Referring to the embodiment shown diagrammatically in the drawing, the catheter of the invention will now be

explained in further detail. In the drawing:

Fig. 1    shows a first embodiment of the catheter of the  
10   invention, in longitudinal section;

Fig. 2    shows, on a larger scale, a cross section along the line II-II of Fig. 1;

Fig. 3    shows a second embodiment of the catheter of the invention, in longitudinal section;

15   Fig. 4   shows, on a larger scale, a cross section along the line IV-IV of Fig. 3;

Fig. 5    shows, in the manner of Figs. 2 and 4, a third embodiment of the catheter in accordance with the invention; and

20   Fig. 6   shows, in a cross section, a fourth embodiment of a catheter in accordance with the invention.

Figs. 1 and 2 show a catheter 1 which is provided with a tube 2 having a first channel 3, a second channel 4, a third channel 5, and a fourth channel 6. On the tube 2  
25   there are provided inflatable centering balloons 7 which are arranged fast and sealed-off one behind the other, they being surrounded by a recanalization balloon 8 which is also inflatable and the ends of which are also fastened firmly and sealed-off on the tube 2.

30           The first channel 3 is intended for the conducting of a radioactive element (not further shown) having a generally elongated shape, the length of the radioactive element being adapted to the length of the part of the blood vessel to be irradiated which has been  
35   previously subjected to the recanalization treatment, and the cross section of the radioactive element is adapted to the cross section of the first channel 3, all in such a

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manner that the radioactive element can be brought guided  
displaceably through the first channel 3 to and from the  
irradiation position. For this purpose, the radioactive  
element can be fastened to the end of a transport wire  
5 which is also to be displaced through the first channel 3.  
The first channel 3 has a closed distal end which can serve  
as stop surface for the precise positioning of the  
radioactive element.

The second channel 4 is intended for the  
10 receiving and passage of another guide wire, not shown but  
generally known, which, upon the introduction of the  
catheter 1, is first pushed in and through the blood vessel  
and over which the catheter is pushed. In this connection,  
it is pointed out that various techniques are known for  
15 introducing a balloon catheter into a blood vessel. As  
first technique, mention may be made of the so-called  
fixed-wire system, also known as the "on-the-wire system".  
A second technique is the so-called "over-the-wire"  
technique, in which the balloon catheter can be shoved over  
20 the guide wire and displaced. In accordance with a third  
technique, use is made of a balloon catheter, a relatively  
short segment of which is provided  
with a channel having an inlet and an outlet, the guide  
wire extending through this channel so that the catheter  
25 can be pushed along the guide wire. This last technique is  
generally referred to as the monorail system. This monorail  
system is also preferably, but not strictly necessarily,  
used in catheters in accordance with the present invention.  
In the embodiment shown in Fig. 1, the channel 4 makes the  
30 catheter suitable for use of the monorail technique. The  
second channel 4, in front of and behind the places where  
the recanalization balloon 8 is connected to the tube 2 is  
provided with openings 9 which connect the second channel  
4 with the surroundings, that is to say, when the catheter  
35 is introduced, with the inside of the blood vessel treated.  
Furthermore, the second channel 4 does not extend over the  
entire length of the tube 2, but from the distal end of the



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tube 2 where the second channel 4 terminates in an open mouth 10, up to and some distance past the openings 9 located furthest from the open mouth 10.

5       The third channel 5 (Fig. 2) is intended for the feeding of fluid by gas and/or liquid to the recanalization balloon 8. For this purpose, openings are present in the wall of the tube 2 in the third channel 5 within the recanalization balloon 8 but outside the central balloons 7.

10       The fourth channel 6 (Fig. 2) is intended for the feeding of fluid (that is to say gas and/or liquid) to the centering balloons 7. For this purpose, openings are present in the wall of the tube 2 within each centering balloon.

15       For the performing of a recanalization and irradiation treatment, the guide wire, travelling through the second channel 4 with its distal end extending past the open mouth 10 is inserted into the blood vessel and guided therein in the customary, known manner in the direction of  
20       the blood vessel wall to be treated. The catheter 1 is inserted, with balloons 7 and 8 uninflated, through the same opening as the guide wire in the blood vessel and follows the guide wire upon the further displacement. After the distal end of the catheter has thus been brought to the  
25       desired place, the guide wire can, if desired, be withdrawn to past the openings 9 located furthest from the open mouth 10, as a result of which the circulation of blood through the blood vessel can take place undisturbed to a far-reaching extent. Furthermore, via the third channel 5,  
30       fluid is fed for the inflating of the recanalization balloon 8 for the carrying out of the first phase of the treatment -- the stretching of the blood vessel. After this has been done, the fluid fed is discharged again via channel 5 and fluid is fed via the fourth channel 6 for the  
35       inflating of the centering balloons 7 whereby, as can be noted from Fig. 2, the tube 2 is so positioned in the blood vessel that the center line of the first channel 3 is

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centered in the centering balloons and thus also positioned in the blood vessel. The catheter 1 is then in an optimal condition of irradiation. The irradiation is effected by displacing the radioactive element through the first  
5 channel 3 until it comes against the end of the first channel 3 and, after being held in place for the desired period of time, is pulled back again and removed from the body of said radioactive element. Finally, after allowing the balloons to empty, the catheter is removed and the  
10 treatment is completed.

In Fig. 3 and 4, a catheter 11 is shown which is provided with a tube 12 having a first channel 13, a second channel 14, and a third channel 15. Around the tube 12, at the distal end thereof, there is arranged a recanalization  
15 balloon 18 which, as customary, has an elongated shape and is connected at its ends firmly and in sealed fashion to the tube 12. Between the tube 12 and the recanalization balloon 18 there extends a centering means in the form of a strip 17 of a thin flexible material extending helically  
20 around the tube 12. The width of the strip 17 agrees with the distance between the tube 12 and the recanalization balloon 18 in inflated state. The strip 17 is fastened to both the tube 12 and to the recanalization balloon 18.

The first channel 13 is intended for the guiding  
25 of a radioactive element (any further) of the same type as already described above. Like the first channel 3 in Fig. 1,

the first channel 13 has a closed distal end which can serve as stop surface for the accurate positioning of the  
30 radioactive element. The second channel 14 is intended for the receiving and passage of a guide wire, not shown any further but generally known. The second channel 14 is provided, in front of and behind the places where the recanalization balloon 8 is connected to the tube 2, with  
35 openings which connect the second channel 4 with the surroundings, that is to say, when the catheter is present, with the inside of the blood vessel treated. Said openings

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are present in Fig. 3 behind the plane of the drawing and have the same function as the openings 9 in the catheter 1 of Figs. 1 and 2. The third channel 13 (Fig. 4) is intended for the feeding of fluid to the recanalization balloon 18.

5 For this purpose, openings (not shown) are provided in the wall of the tube 12 in the third channel 15 within the recanalization balloon 8. In view of the fact that the strip 17 extends helically around the tube 12, in principle one opening should be sufficient. Of course, it is also

10 possible to apply more than one strip 17, in which case each screw thread thus formed must be able to be fed with fluid in order to be able to carry out the recanalization treatment in the manner desired, which can be effected in a manner similar to that described above in connection with

15 the catheter of Figs. 1 and 2. In this connection, the centering function of the centering balloons 7 in the case of the catheter 1 will be taken over in the case of catheter 11 by the strip 17 which, upon the inflation of the recanalization balloon 18, assume the helical position

20 extending perpendicular to the tube 12 and the wall of the recanalization balloon 18 and in this way, as shown in Fig. 4, centers the axis of the first channel 13 with respect to the recanalization balloon 18 and therefore the wall of the blood vessel to be treated.

25 It is pointed out that in the event that two strips 17 are arranged within the recanalization balloon 18, as well as use is made of a tube 2 such as shown in Figs. 1 and 2 in which the one screw thread within the recanalization balloon 18 is fed by the third channel 5 and

30 the other screw thread by the fourth channel 6 in the tube 2, it is possible, after the recanalization treatment, to relieve one of the screw threads of the fluid pressure or even bring it under a slight vacuum, as a result of which a helical passage is created around the outside of the

35 recanalization balloon for the circulation of the blood through the blood vessel. If desired, one or the other screw thread can alternately perform the passage function.

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Fig. 5 shows in cross section a catheter 21 which is substantially identical to that of Figs. 3 and 4, as can be noted from the identical reference numerals. The difference is that in this embodiment the strip 17 is replaced by thread-shaped elements 27 which are connected on one side to the tube 12 and on the other side to the recanalization balloon 18. Upon the inflation of the recanalization balloon 18, the thread-shaped elements 27 will center the axis of the first channel 13 with respect to the recanalization balloon 18 and in this way the blood vessel wall to be treated.

Fig. 6 shows, diagrammatically in cross section, an embodiment of a catheter in accordance with the invention in which the centering means, in the same way as in the embodiment of Fig. 1, comprise a plurality of balloons. The centering balloons of the embodiment shown in Fig. 6 are, however, not arranged one behind the other in the longitudinal direction of the catheter as in Fig. 1, but are radially distributed around the central tube 30. Fig. 6 shows six centering balloons 32 to and including 37 which are arranged within a recanalization balloon 31 around the central tube 30. The centering balloons have an elongated shape with a length which is as great as that covered by the recanalization balloon or at least a considerable part thereof. In the example shown, the elongated centering balloons can be inflated via the channels 5 and 6, which are provided for this purpose with transverse holes 5a, 5b, 5c and 6a, 6b, 6c respectively. The elongated balloons lie radially around the tube 2. Since, however, the channel 3 which serves for the guiding of the radioactive element is not centered in the tube, the diameter of the elongated balloons is varied in accordance with whether they are closer to or further from the channel 3, so that the centering balloons in inflated state accurately center the channel 3 with respect to the recanalization balloon 31 which lies against the wall of the blood vessel. It is pointed that each elongated balloon

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may be a combination of a number of balloons located one behind the other.

It is obvious that, within the scope of the invention as set forth in the accompanying claims, a large number of modifications and variants are furthermore possible. Thus the first channel can also be used for the feeding of fluid to the balloons, so that the third and/or fourth channels could be dispensed with. In this connection, it could be that the first channel is not used during the recanalization treatment so that it is available for the feeding of fluid under pressure to the recanalization balloon. If no pressure is desired in the first channel during the transporting of the radioactive element, then a separate channel may be present in the embodiment with the centering balloons or the double screw thread for the operating of the centering means. Furthermore, the first channel could be used for the guide wire, since guide wire and radioactive element are not used at the same time. This possibility, however, is less preferable since the first channel must then be open at its distal end and the radioactive element may come into contact with blood.

Furthermore, depending on the intended use of the catheter, the second channel 4 or 14 can be located exclusively in the front end of the catheter, that is to say between the balloon means and the distal end. These and similar modifications are obvious to those skilled in the art.

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## Claims

1. A catheter comprising an elongated tube having a first channel for the guiding of a radioactive element and a second channel for the passage of a guide wire for the catheter, the elongated tube being provided with temporarily activatable centering means on its outer circumference near its distal end, characterized in that the centering means are surrounded by a recanalization balloon which is inflatable by fluid fed via a third channel so as to form an elongated body, and in that the centering means are activatable within the recanalization balloon.

2. A catheter according to Claim 1, characterized in that the centering means are activated by the inflation of the recanalization balloon.

3. A catheter according to Claim 2, characterized in that the centering means are connected on the one hand to the recanalization balloon and on the other hand to the tube, all in such a manner that the tube is centered in the recanalization balloon upon the inflation thereof.

4. A catheter according to Claim 2 or 3, characterized in that the centering means comprise inflatable balloon means which are inflatable by fluid fed via the third channel, the balloon means comprising a number of balloons which center the part of the first channel extending between the balloons with respect to the outer circumference of the recanalization balloon.

5. A catheter according to Claim 1, characterized in that the centering means are activatable independently of the inflation of the recanalization balloon.

6. A catheter according to Claim 5, characterized in

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that the centering means comprise inflatable balloon means which are inflatable via fluid fed via at least one fourth channel arranged in the tube, the balloon means comprising a number of balloons which center the part of the first  
5 channel extending between the first and the last balloons with respect to the outer circumference of the recanalization balloon.

7. A catheter according to any of Claims 4 to and including 6, characterized in that the balloon means  
10 comprise a plurality of balloons which are arranged one behind the other in the longitudinal direction of the tube within the recanalization balloon.

8. A catheter according to any of Claims 4 to and including 6, characterized in that the balloon means  
15 comprise a number of elongated balloons which are arranged alongside of each other radially around the tube with the longitudinal axis parallel to that of the tube.

9. A catheter according to Claim 8, characterized in that the elongated balloons have a diameter which is  
20 adapted to the radial position of the corresponding balloon with respect to the tube.

10. A catheter according to Claim 8 or 9, characterized in that the elongated balloons have a length which amounts to at least a considerable part of the length  
25 of the recanalization balloon.

11. A catheter according to any of Claims 7 to and including 10, characterized in that one or more elongated balloons are formed by a plurality of balloons located one behind the other.

30 12. A catheter according to any one of the preceding claims, characterized in that a further channel is present

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which extends from a distal place past the recanalization balloon and the centering means to past the proximal end of the recanalization balloon and the centering means and is provided on opposite sides of the recanalization balloon and the centering means with at least one connecting opening with the surroundings.

13. A catheter according to Claim 12, characterized in that the further channel coincides with the second channel, in which connection the guide wire can be pulled back further from the distal end of the second channel therein than the proximal connecting opening or openings.

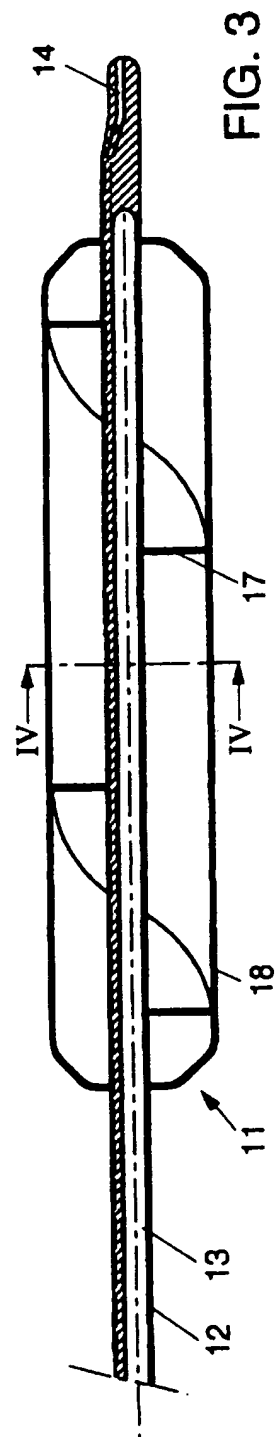
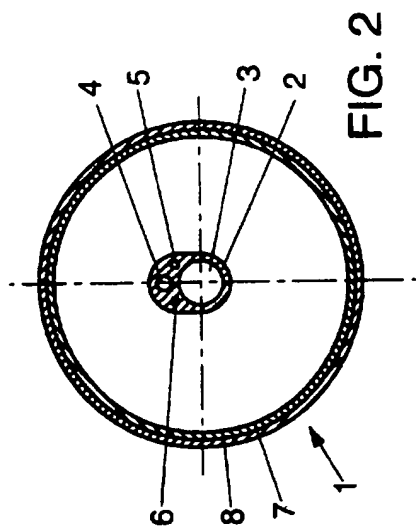
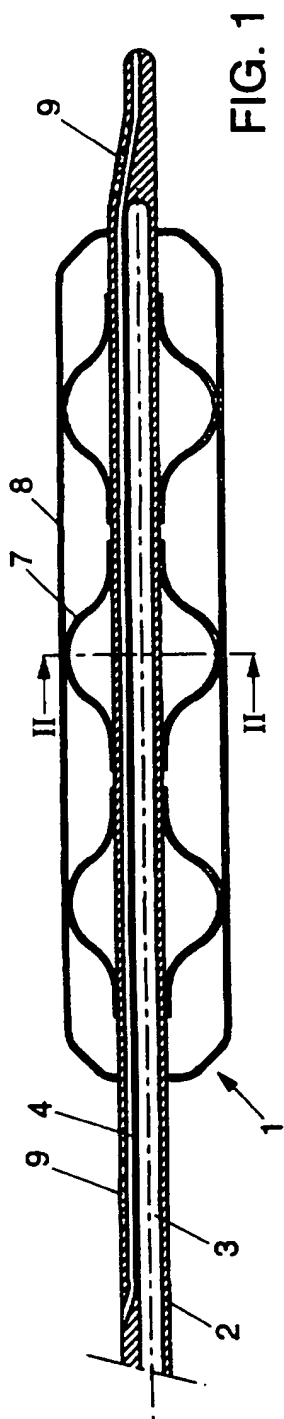
14. A catheter according to any of Claims 4 to and including 11, characterized in that the balloon means comprise a number of balloon parts which are independent of each other, each of which is in communication with the third channel.

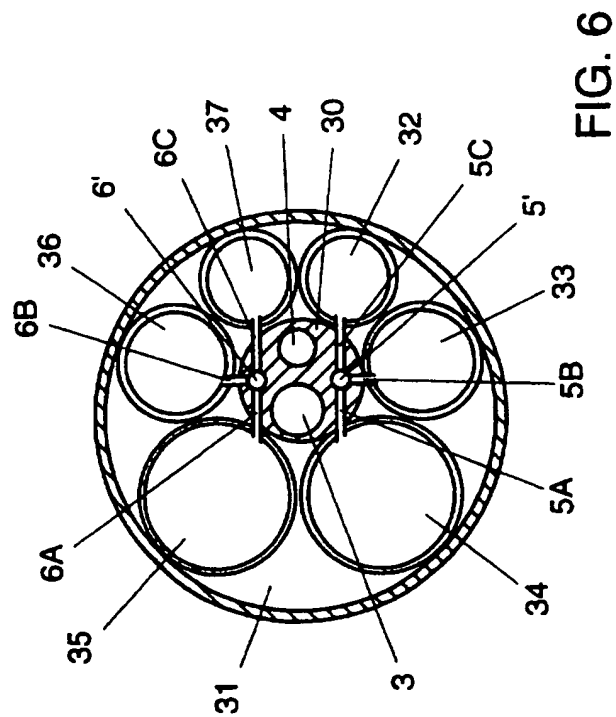
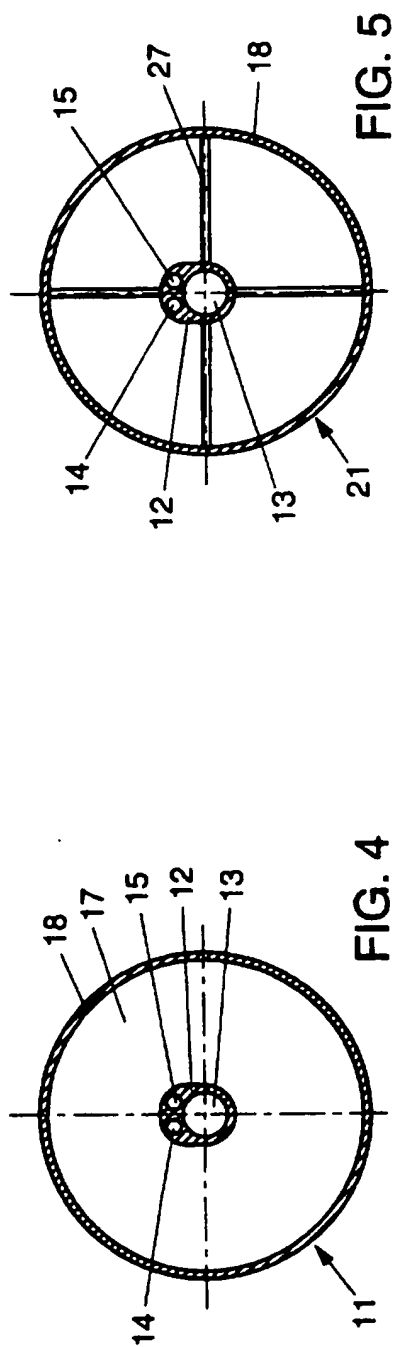
15. A catheter according to any of Claims 4 to and including 11, characterized in that the balloon means comprise a plurality of balloon parts which are independent of each other, each of which is connected with the tube and each of which is in communication with the fourth channel.

16. A catheter according to any one of the preceding claims, characterized in that if the axis of the first channel does not coincide with the longitudinal axis of the tube, the centering means are so shaped that after the activation thereof, the axis of the first channel coincides with the longitudinal axis of the centering means.

17. A catheter according to any one of Claims 1 to and including 12, or 14 to and including 16, characterized in that the second channel extends from a distal place past the recanalization balloon to or close to the distal end of the tube.







## INTERNATIONAL SEARCH REPORT

Internat. J. Application No.

PCT/NL 97/00384

A. CLASSIFICATION OF SUBJECT MATTER  
 IPC 6 A61N5/10 A61M25/10

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61N A61M

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## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	WO 96 06654 A (TEIRSTEIN) 7 March 1996 see abstract; figures ---	1-3
Y	EP 0 330 376 A (BARD) 30 August 1989 see column 11, line 33 - line 39; figures ---	1-3
A	EP 0 567 788 A (INDIANA UNIVERSITY) 3 November 1993 see abstract; figures ---	1
A	WO 96 14898 A (OMNITRON INTERNATIONAL) 23 May 1996 see claim 1; figures ---	1
A	WO 95 26681 A (LIPRIE) 12 October 1995 see abstract; figures 1-5 ---	1
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Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 4 781 681 A (SHARROW) 1 November 1988 see abstract; figures 2,6 ---	1
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